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Fabricating optical lenses by inkjet printing and heat-assisted *in situ* curing of polydimethylsiloxane for smartphone microscopy

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Abstract. We present a highly repeatable, lithography-free and mold-free method for fabricating flexible optical lenses by *in situ* curing liquid polydimethylsiloxane droplets on a preheated smooth surface with an inkjet printing process. This method enables us to fabricate lenses with a focal length as short as 5.6 mm, which can be controlled by varying the droplet volume and the temperature of the preheated surface. Furthermore, the lens can be attached to a smartphone camera without any accessories and can produce high-resolution (1 μm) images for microscopy applications. © The Authors. Published by SPIE under a Creative Commons Attribution 3.0 Unported License. Distribution or reproduction of this work in whole or in part requires full attribution of the original publication, including its DOI. [DOI: [10.1117/1.JBO.20.4.047005](https://doi.org/10.1117/1.JBO.20.4.047005)]

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1 Introduction

Traditional lenses are constructed by mechanical polishing or injection molding of rigid materials such as glass or plastics. The high optical quality lens surface requires well-controlled fabrication parameters, which increase complexity and operating costs.¹ In contrast, lens formation due to surface energy minimization, such as liquid lenses, has provided an alternative method for creating small lenses of high quality without the requirement of molds or complex parameter control.² However, freely flowing liquid lenses require a system to provide mechanical stability and prevent evaporation.³ In contrast, lenses can be fabricated by curing liquid polymers to set the lens profile permanently. For example, microlenses with focal lengths on the order of 1 mm have been fabricated by photoresist reflow. Small lenses with millimeter-range focal length are highly applicable to commercial electronics, such as smartphones and digital cameras.

Polydimethylsiloxane (PDMS) is optically transparent ($T > 95\%$) in the visible spectrum with a high refractive index ($n \sim 1.47$) and displays minimal yellowing over time.⁴ PDMS has been employed to construct microfluidic devices since the 1990s,⁵ and still maintains its wide applicability to date.^{6–10} As a lens material, three types of fabrication techniques have been adopted: (1) lithographic methods,¹¹ (2) surface tension driven methods,¹² and (3) embossing methods.¹³ These current approaches demonstrate the feasibility of creating PDMS lenses with good optical characteristics and reproducibility; however, they either require time-consuming fabrication procedures typically measured in hours, or have high costs due to lithographic and molding equipment required, and generally limit the size of the lens to the micrometer scale.^{12,14} A recently

introduced method of creating PDMS lens by gravity-assisted hanging droplet formation has both the advantage of low cost and good optical quality; however, the process requires iterative drop-bake cycles to achieve the desired focal length.¹⁵

In this paper, we describe a method to fabricate lenses by inkjet printing of PDMS droplets on a heated surface. The small PDMS droplet is released at a prescribed height from the inkjet print head. Upon impacting the surface, the rather complex interactions of kinetic and surface energy, inertia, gravity, and fluid viscosity cause the droplet to take a plano-convex shape. The printing procedure is robust and can be performed without cleanroom facilities. The rest of the paper is outlined here. In Sec. 2, we describe the rationale behind forming lenses by *in situ* curing. In Sec. 3, we demonstrate the printing method to fabricate the lenses and discuss characterization results. As an application, we show that our lens can transform a smartphone camera into a microscope by simply attaching the lens without any supporting attachments or mechanism. The strong, yet non-permanent adhesion between PDMS and glass allows the lens to be easily detached or replaced after use. An imaging resolution of 1 μm with an optical magnification of 120 \times has been achieved.

2 Concept

When a drop of water is deposited onto a surface, the minimization of interfacial surface energies produces a very smooth and curved surface that can be used as a lens. Likewise, an uncured PDMS droplet can also form a liquid lens. However, the rheological properties of PDMS cause a deposited droplet to flow into a thin pancake shape with little lensing effect. As PDMS is a thermally curable elastomer, the droplet deformation can be intervened by heat accelerated curing *in situ*. The rapid heating causes the droplet to cure and stop further deformation, thereby preventing excess spreading and retaining significant

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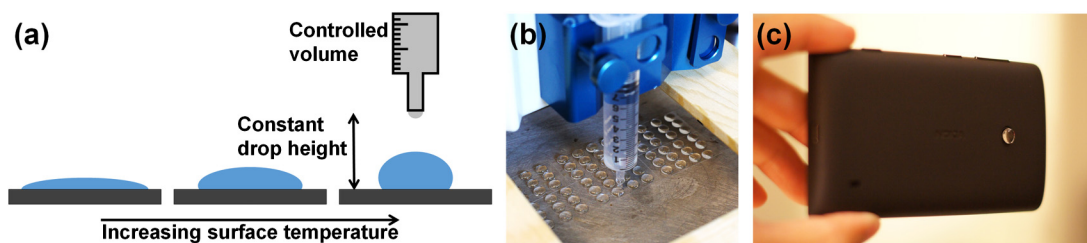


Fig. 1 Fabrication and application of polydimethylsiloxane (PDMS) lens: (a) changing the temperature of the preheated surface modifies the geometry of a cured PDMS droplet, (b) the PDMS inkjet print head printing droplet lenses on a heated surface, and (c) the lens can be nonpermanently attached onto a smartphone for microscopy applications.

surface curvature, as shown in Fig. 1(a). By controlling both the volume of the droplet and the preheated surface temperature beneath the droplet, the curing speed can be controlled, which subsequently controls the droplet's surface curvature and the focal length. The PDMS inkjet print head, as shown in Fig. 1(b), allows us to test these two variables. The PDMS lens can be nonpermanently attached onto a smartphone, as shown in Fig. 1(c), for microscopy applications.

3 Design and Experiment

PDMS solution (Sylgard 184, Dow Corning) was prepared by mixing manufacture recommended proportions of PDMS base and curing agent by a weight ratio of 10:1. After mixing and vacuum bubble removal, an inkjet printing system was set up by incorporating a computer programmable syringe pump with the ability to print with PDMS ink, suspended on a semi-automated stage placed a constant and controlled height above a temperature-controllable hotplate, as shown in Fig. 1(b).

3.1 Temperature-Controlled *In Situ* PDMS Lens Formation

To prepare a preheated surface, a coverslip was cleaned and placed atop a hotplate. 50 μL of PDMS was dropped on the coverslip from a 20 mm height with the print head, as demonstrated in Figs. 1(a) and 1(b). PDMS cures at room temperature, but

exhibits accelerated curing with increasing temperatures. The procedure was repeated with temperature increments of 20°C, from 60 up to 200°C.

At lower temperatures, PDMS droplets require a longer time to cure (roughly 350 s at 60°C), allowing the viscous liquid to spread across the surface as gravity pulls the liquid toward the surface. The viscosity of the uncured PDMS increases as the curing process starts, and an equilibrium is attained when the viscous forces balance out the gravitational force. This forms a very thin, flat lens with negligible curvature and little optical power. In contrast, heat-accelerated curing solidifies the liquid droplet *in situ*, in effect stopping the spreading process. This limits the droplet to spread into a smaller diameter and at the same time, retains significant surface curvature effective for refractive ray bending.

Figure 2 shows the morphological evolution of 50 μL droplets during *in situ* curing at 80 and 200°C. At 80°C, it can be seen that the initial droplet spread is wider and continues to flow out into a thin shape before curing completes at ~ 80 s after dispensing. At 200°C, the PDMS droplet virtually cures on contact, causing significant curvature. No burning or charring was observed at these temperatures. Side views of droplets cured at 60 to 200°C are shown in Fig. 3 for comparison. It is seen that as the surface temperature increases, the time required for droplet curing decreases, the flow of the droplet is limited, and the subsequent droplet

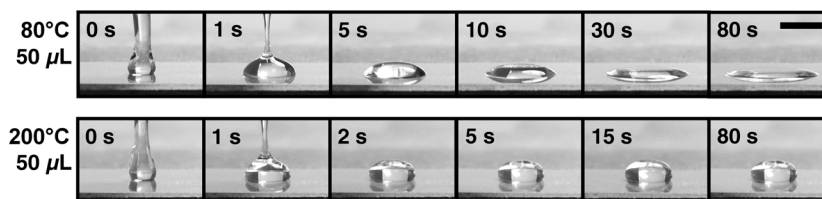


Fig. 2 Morphological evolution of PDMS droplet cured at (a) 80°C and (b) 200°C. While the 80°C droplet flows into a thin pancake shape with time, the 200°C droplet attains its final shape at 2 s. Scale bar is 5 mm.

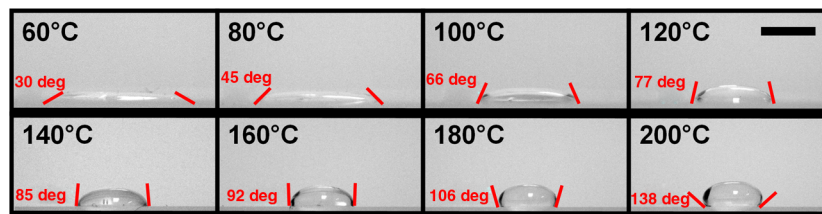


Fig. 3 Side view of PDMS droplets (50 μL) deposited onto a surface at various temperatures. Scale bar is 5 mm.

exhibits a decreased diameter, increased height, and increased surface contact angle, thus forming a smaller radius of curvature which leads to a higher optical power.

3.2 Volume-Controlled In Situ PDMS Lens Formation

To investigate the relationship between focal length and droplet volume, the hotplate was set to a constant temperature of 200°C and different volumes of PDMS were deposited on the surface while all other conditions remained identical. Volumes of 10 to 200 μL were used, respectively, with the resulting side views and geometrical measurements shown in Fig. 4. As the droplet volume increases, the lens diameter increases intuitively; however, the contact angle only varies within $\pm 4.4\%$. The center portion of the lens is found to exhibit decreasing curvature and eventually flattens for increasing volume. This limitation makes it difficult to create high-magnification lenses >1 cm in diameter using this method.

The properties of the lens are determined by its geometric parameters. Since the curing temperature of PDMS determines the speed of polymerization, and thus the contact angle and diameter of the lens droplet, the focal length of the lens can be accurately tuned in a single step. Similar to other liquid lenses, the droplet experiences uniform surface forces from all sides during curing, which greatly eliminates surface roughness.

3.3 Printing Repeatability

To demonstrate the repeatability of the inkjet printing technique in fabricating lenses, 20 lenses were made for each volume of 10, 25, 50, 75, and 100 μL , at each temperature between 100 and 200°C. Due to limited hotplate area, only five lenses were made for the volumes >100 μL due to their larger size. Figure 5 shows the trend of the lens diameter with respect to the lens volume and curing temperature. It is observed that for volumes <100 μL , the diameter deviated $<5\%$ in all cases, but was generally controlled within 2.7% in most cases.

3.4 Optical Characterization of Lenses Cured at 200°C

From the preceding sections, it is shown that at a certain fixed hotplate temperature, decreasing the droplet volume creates a smaller droplet with a smaller radius of curvature, or a shorter focal length. As the PDMS lenses cured at 200°C have the smallest diameter, we next characterized the focal lengths of the sequence of different volume lenses cured at 200°C.

The setup to characterize the focal length is shown in Fig. 6(a). The output from a fiber-coupled diode laser (Newport Model 505 laser diode driver connected to fiber

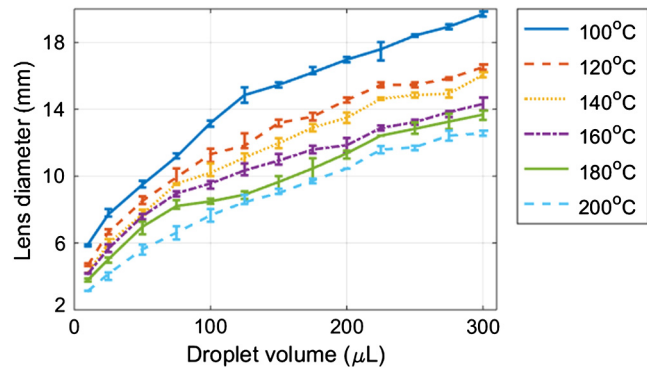


Fig. 5 Lens diameter as a function of various lens volumes and curing temperatures. The line indicates the mean, while the upper and lower limits of the error bar indicate the diameter deviation.

pigtailed laser diode LD-635-31A) was passed through a convex lens (L1) (Thorlabs LA1131-ML) with a focal length of 50 mm, a neutral density filter (ND) (Thorlabs ND10A), an iris (I) (Thorlabs ID25/M), and a glass slide (G) on which the PDMS lens (L2) was attached. A CCD camera (Amscope MT 300, Amscope) with a pixel size of 1.2 μm was affixed on a micrometer stage with a travel range of ~ 5 mm from the PDMS lens. The error with the stage measurement was ~ 0.05 mm. For PDMS lenses with a focal length >10 mm, the micrometer stage was removed, the CCD camera was positioned manually with a ruler and the associated error was ~ 1 mm.

Figure 6(b) shows the laser beam spot captured on the CCD camera with the 10 μL lens. The image has been transformed into gray scale before intensity analysis with MATLAB® (Mathworks). The beam intensity profiles along the vertical and horizontal directions are also shown. The images were captured at 5.4, 5.6, and 5.8 mm distances. The focal length is found to be 5.6 mm, where the full-width half-maximum of the point spread function is captured as the minimum with the CCD camera. Figure 6(c) shows the comparison of the focal length of lenses created with various droplet volumes at 200°C. The focal lengths for volumes of 10, 25, 50, 75, 100, 125, 150, 175, and 200 μL were 5.6 ± 0.05 , 6.3 ± 0.05 , 6.7 ± 0.05 , 8.6 ± 0.05 , 10 ± 1 , 15 ± 1 , 30 ± 1 , 62 ± 1 , and 84 ± 1 mm, respectively.

The optical power of a convex lens is the degree to which it converges light and can be expressed by the equation $P = 1/f$, where P is the power of the lens and f is the focal length. The numerical aperture of a lens is commonly expressed as $NA = n \sin \theta$, where n is the index of refraction of the medium in which the lens is working ($n_{\text{air}} = 1$) and θ is the half-angle of the maximum cone of light that can enter or exit the lens. For the

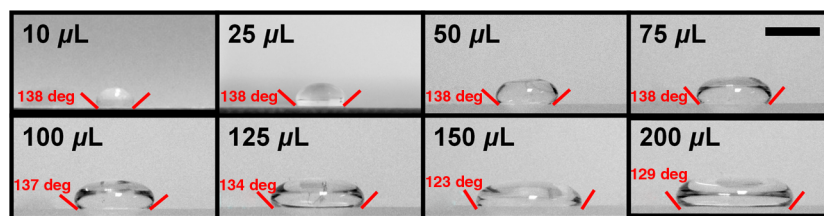


Fig. 4 Side view of PDMS droplets (various volumes) deposited onto a surface at 200°C temperature. Scale bar is 5 mm.

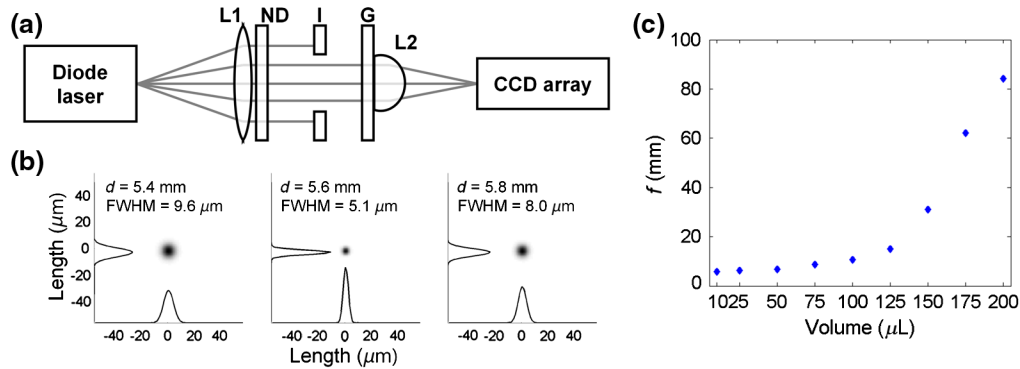


Fig. 6 Determining the focal length of the PDMS lenses. (a) Schematic of optical path; optical path of diverging diode laser enters a convex lens with 40 mm focal length (L1), a neutral density filter (ND), a glass slide (G) for support, and the PDMS lens (L2); the focused beam is captured by the CCD camera. (b) CCD camera image showing beam intensity profile when tested with the 10 μL , 200°C lens, at distance of 6.0, 6.3, and 6.6 mm, respectively. (c) The trend of focal length with different lens volumes from 10 to 200 μL .

PDMS lens with a focal length of 5.6 mm (10 μL cured at 200°C), the optical power was found to be $\sim 180 \text{ m}^{-1}$. The lens has a usable radius of 1.02 mm, and the half-angle is found to be 10.32 deg, leading to an NA of ~ 0.27 . Future work is needed to fully characterize the lens surface curvature for a more accurate NA estimate.

3.5 Minimum Resolvable Feature Size

Add-on accessories to turn a smartphone into a microscopic imaging device are widely available; however, most of these attachments are bulky or require device-specific attachment components.¹⁶ To demonstrate a practical application, the PDMS lens (10 μL cured at 200°C) was attached to a Nokia Lumia 520 budget smartphone camera (Microsoft, Richmond, Virginia) as shown in Fig. 1(c). The camera has a 5-megapixel sensor and the minimum focus distance of the smartphone camera is 10 cm as specified by the manufacturer. The adhesive

property of PDMS on glass and plastic surfaces allowed the PDMS lens to be attached nonpermanently onto the camera window without additional support and was able to be used in our experiments for at least 30 min at a time without falling off. The effective focusing distance of the smartphone with the PDMS lens was ~ 5 mm.

In order to determine the minimum resolvable feature size of the smartphone-PDMS lens system, a binary spoke target with a minimum feature size of 1 μm was imaged. The spoke target was manufactured commercially using electron beam lithography with chrome on glass, as shown in Fig. 7. The central portion of the target was imaged with an Olympus IX-70 (Olympus Corp) microscope with 400 \times magnification, as shown in Fig. 7(a). The image obtained by the smartphone-PDMS lens system with a separate backlight source is shown in Fig. 7(b). The width of the 64 spokes decrease linearly from 300 μm from the outer rim to 1 μm at the inner rim. Intensity profiles of the images were obtained using MATLAB[®].

A perfect reproduction of the spoke target pattern would yield an intensity represented by a square wave with 64 cycles, each with the highest intensity at 256 bits and the lowest intensity of 0 bits. Fringe visibility (V) quantifies the contrast of interference of the optical system and is defined as $(I_{\text{max}} - I_{\text{min}})/(I_{\text{max}} + I_{\text{min}})$. An ideal output yields a visibility of 1, while a featureless output yields a visibility of 0. For a 256 bit mask function, where $I_{\text{max}} = 256$ bit and $I_{\text{min}} = 0$ bit, visibility = 1. The respective maximum and minimum intensities and fringe visibility obtained for different spoke

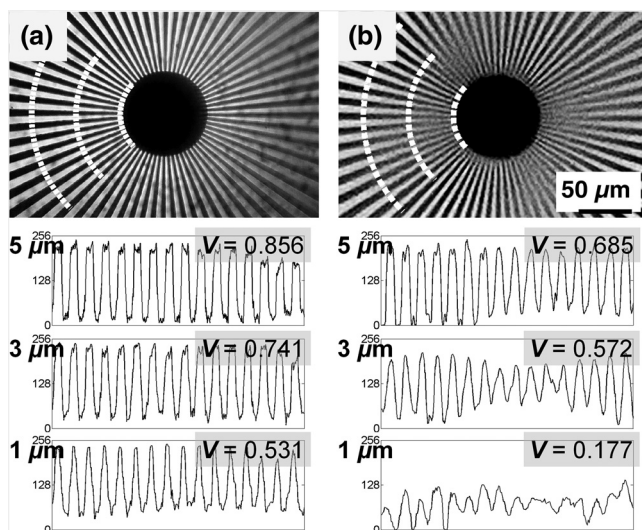


Fig. 7 Determining minimum resolvable feature size by imaging a 1 μm minimum line width binary spoke target: (a) obtained with 400 \times microscope and (b) obtained with a smartphone with a 10 μL , 200°C PDMS lens. The three line sections, respectively, indicate the region where the spoke widths are 5, 3, and 1 μm . V , fringe visibility.

Table 1 Intensity and fringe visibility of spoke target image.

Imaged with	Microscope			Polydimethylsiloxane lens		
	5	3	1	5	3	1
I_{max} (bit)	220	216	219	225	195	103
I_{min} (bit)	17	32	67	42	53	72
Fringe visibility	0.86	0.74	0.53	0.69	0.57	0.18

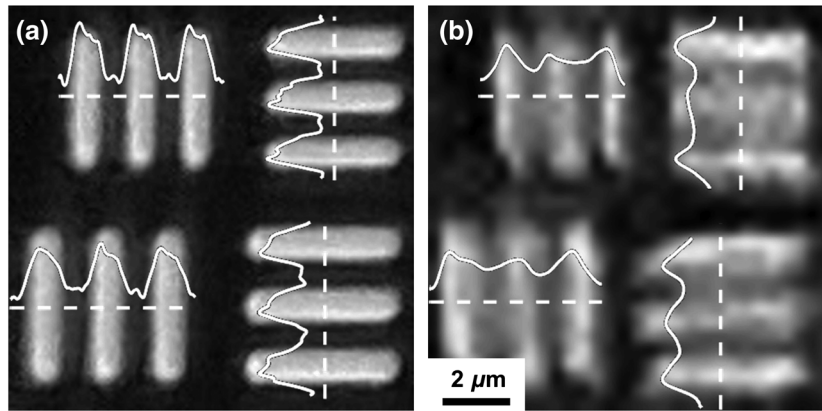


Fig. 8 Determining minimum resolvable feature size by imaging a USAF 1951 resolution test target with line widths of $1.10\ \mu\text{m}$ (top patterns) and $1.23\ \mu\text{m}$ (bottom patterns): (a) obtained with $400\times$ microscope and (b) obtained with a smartphone with a $10\ \mu\text{L}$, 200°C PDMS lens.

line widths from the microscope and smartphone-PDMS lens system are summarized in Table 1.

The visibility of the $1\ \mu\text{m}$ pattern from the smartphone-PDMS lens system is lower than that of the microscope; however, the intensity map indicates that 62 of 64 patterns can be resolved. It is important to note that the imaging contrast highly depends on the camera hardware, and internal processing

Table 2 Intensity and fringe visibility of USAF 1951 resolution test target image.

Imaged with	Microscope		Polydimethylsiloxane lens					
Linewidth (μm)	1.23III	1.23≡	1.10III	1.10≡	1.23III	1.23≡	1.10III	1.10≡
I_{max} (bit)	206	210	204	196	138	136	132	138
I_{min} (bit)	51	60	39	50	76	74	82	95
Fringe visibility	0.60	0.56	0.68	0.59	0.29	0.30	0.23	0.18

performed by the smartphone may have an important role in determining the minimum resolution of the system. A higher-end smartphone camera may yield better results than those obtained for this analysis.

A further resolution test was performed using a standard USAF 1951 resolution test target (#58-198 Edmund Optics Inc.), in order to prevent radially symmetric distortions from affecting the previous method of resolution determination. The target was separately imaged using a microscope with $400\times$ magnification, as shown in Fig. 8(a), and the smartphone-PDMS lens system with a separate backlight source, as shown in Fig. 8(b). The USAF patterns selected are, respectively, from group 8 element 6 vertical and horizontal (top), and group 8 element 5 vertical and horizontal (bottom), yielding a respective line width of 1.10 and $1.23\ \mu\text{m}$. The dotted lines indicate the region of the pattern from where the light intensity was obtained.

Fringe visibility was calculated for each pattern and summarized in Table 2. It is seen that the visibility of the 1.23 and $1.10\ \mu\text{m}$ test patterns from the smartphone-PDMS lens system remains lower than that of the microscope; however, the

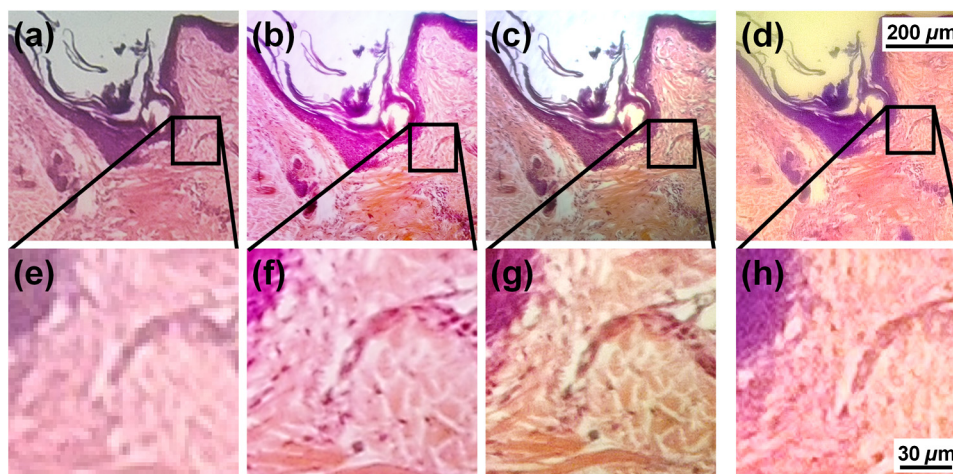


Fig. 9 Comparison of human skin and hair follicle cross-section histology slide. (a), (b), (c), and (d) are, respectively, imaged with an Olympus IX-70 microscope at $40\times$ magnification, $100\times$ magnification, $200\times$ magnification, and with a Nokia Lumia 520 smartphone with PDMS lens system. (d), (e), (f), and (g) show the magnified regions, respectively.

intensity map clearly displays the three peak patterns. The minimum resolvable feature and fringe visibility is comparable to that performed using the binary spoke target.

3.6 Smartphone Microscopy Application

Figure 9 demonstrates the potential of the smartphone-PDMS lens system to be used in biological and biomedical research. A cross-section of a human skin-hair follicle histological slide (AmScope) was employed, and the image captured by an Olympus IX-70 microscope was compared with that by the smartphone-PDMS lens system. Figures 9(a), 9(b), and 9(c) show the sample imaged under the microscope at 40 \times , 100 \times , and 200 \times , respectively, while Fig. 9(d) shows the same sample imaged with the smartphone-PDMS lens system. A magnified inset of each image is shown in Figs. 9(e) to 9(h). It can be seen that with the smartphone-PDMS lens system, individual skin cells can be observed.

The base magnification of the lens was found to be 120 \times by comparing the observed size of an arbitrary structure in a clearly focused image taken with the smartphone and the aforementioned microscope. The magnification of the smartphone with PDMS lens can be further enhanced by combining software based digital magnification.

4 Conclusion

In this paper, we describe an inkjet printing technique to fabricate optical lenses by *in situ* curing PDMS droplets of controlled volume and at controlled temperature. This single-step method allows lenses with different focal lengths to be made by varying the droplet volume and surface temperature. The semiautomated printing technique is highly scalable for lenses of different focal lengths and can be modified for parallel fabrication with higher throughput. The material cost of the PDMS was calculated to be <0.01 USD for a 10 μ L lens and can be conveniently attached to a smartphone camera via the strong but nonpermanent adhesion between PDMS and glass. An imaging resolution of 1 μ m and an optical magnification of 120 \times have been demonstrated with a PDMS lens of 5.6 mm focal length attached to a low-cost smartphone. We believe that the simplicity and robustness of this printing process will introduce a new standard for fabricating lenses with various focal lengths without the requirement of large manufacturing facilities. Future work will include fabrication and characterization of smaller lenses that will yield greater magnification but have been difficult to manipulate due to their small sizes.

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Biographies of the other authors are not available.